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## Rapid prototyping of a low-cost graphene-based impedimetric biosensor

Sinziana Popescu<sup>a</sup>, Carl Dale<sup>b</sup>, Neil Keegan<sup>b</sup>, Biswajit Ghosh<sup>c</sup>, Richard Kaner<sup>d</sup>, John Hedley<sup>a</sup>

<sup>a</sup>*School of Mechanical and Systems Engineering, Newcastle University, Newcastle-upon-Tyne, NE1 7RU, United Kingdom*

<sup>b</sup>*Institute of Cellular Medicine, Newcastle University, Newcastle-upon-Tyne, NE2 4HH, United Kingdom*

<sup>c</sup>*School of Energy Studies, Jadavpur University, Kolkata 700 032, India*

<sup>d</sup>*Department of Chemistry and Biochemistry, Los Angeles, CA 90095, United States*

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### Abstract

This paper presents a preliminary investigation towards rapid prototyping of a low-cost biosensor based on reduced graphene oxide (rGO). The devices are fabricated via a laser scribing process and their functionality is demonstrated by their functionalization and subsequent immobilization of 7% bovine serum albumin (BSA). Non-faradaic electrochemical impedance spectroscopy (EIS) indicated a 33-42% decrease in impedance upon immobilization. An electroless nickel deposition process is demonstrated to enable electrical contacts to the device, with optimized plating conditions (pH, temperature) leading to a rGO-nickel contact resistance of 19  $\Omega/\text{mm}^2$ .

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*Keywords:* graphene; reduced graphene oxide; impedimetric biosensor; interdigitated electrode array; electroless nickel deposition

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### 1. Introduction

Since its discovery in 2004 [1], graphene has received significant research attention due to its extraordinary properties [2]. Reduced graphene oxide (rGO) has been shown to be suitable for bio/sensing applications [3,4] due to its chemically active nature based on the presence of surface functional groups. However, large-scale production, effective electrical contacting and specific surface functionalization remain key issues for graphene development towards commercial biosensing applications. This work investigates a novel approach to low-cost rapid prototyping of functionalised graphene interdigitated electrode arrays (IDE) utilizing laser reduced graphene oxide on flexible substrates. To complete the sensor fabrication, a novel approach for low contact resistance interfacing via electroless nickel metallization is proposed.

## 2. Results

The rGO sensing platform, containing 10 parallel rGO electrodes (6 mm long, 0.5 mm wide), was produced by employing a Lightscribe DVD drive (Figure 1A), as reported by El-Kady et al [5]. The material was characterized using XPS and Raman spectroscopy, confirming the efficient reduction of the graphene oxide. The rGO atomic composition consisted of 96% carbon and 4% oxygen species, with a reduction factor of  $\approx 14$ , whilst the Auger peak D-parameter of 20.2 is indicative of the dominant  $sp^2$  domain [6,7]. High resolution helium ion microscopy (HIM) validated the lateral exfoliation of the graphene layers upon the photo-thermal reduction process (Figure 1C). The average rGO sheet was  $300 \Omega/\square$ , measured using a Hall probe station.

The rGO sensing platform was covalently functionalized using carboxyl-reactive EDC-NHS chemistry, which was confirmed using a quantum dot labeling technique. A good distribution of the deposited amino-coated CdSe quantum dots was observed, especially towards the track edges where oxygen species were present. Upon the successful functionalization with EDC-NHS, 7% bovine serum albumin (BSA) was immobilized on the rGO sensing platform. Non-faradaic impedance measurements (phosphate buffered saline PBS, pH 7.5) were taken between successive chemical modification steps. The impedance decreased as a result of the immobilization process (Figure 1B), modelled by the addition of a series capacitive element (in the equivalent circuit). Also, a significant decrease in the equivalent constant phase element was noted whilst the rGO porosity led to an inductive behaviour at high frequencies.

To complete the sensor platform, a two-step electroless nickel deposition was performed on the rGO surface, involving activation (palladium chloride) and deposition in a Ni:P metal bath (nickel sulfate). Optimized bath conditions were determined to be  $65^\circ\text{C}$  and pH of 7.3 for a 2 minute deposition time. The deposited film selectively covered the IDE rGO pads (without the inter-pad GO) and it contained 85% nickel (Figure 1C), quantified with EDX. The contact resistance of nickel onto the rGO was measured using the transmission line method as  $19 \Omega/\text{mm}^2$ .

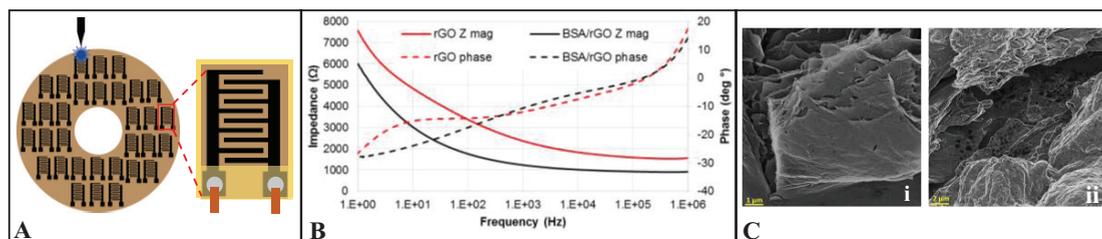


Figure 1: A) Lightscribe rGO production process and IDE diagram; B) Bode plot (impedance magnitude and phase) for the rGO biosensing platform before and after BSA immobilization; C) HIM image of (i) rGO and (ii) rGO after electroless nickel metallization.

## 3. Conclusions

Using the Lightscribe photo-thermal reduction method, rGO IDEs were efficiently manufactured on flexible substrates. The produced rGO showed good electro-chemical properties which are applicable towards biosensing applications and electroless nickel metallization techniques, presenting advantages towards low-cost, low temperature and scalable production of the sensor. Further work will address full biosensor integration and performance characterization.

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